

## Ocean Observation with Opto-Microfluidic Devices

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**ABSTRACT.** The success of ocean observation relies on effective monitoring technologies with increased functionalities, minimized size, and reduced cost. In this study, opto-microfluidic devices for sensing the salinity and temperature of sea water are proposed and demonstrated, which can be prepared with ultrafast laser fabrication and two-photon polymerization techniques. By applying femtosecond lasers as a powerful tool to achieve laser microfabrication with unprecedented high precision and quality, a Mach-Zehnder interferometer (MZI) has been fabricated and integrated into a microchannel as a miniaturized opto-microfluidic system. When the temperature changes or different saline solutions are introduced to the microchannel, different phase shifts in the MZI can be induced. The sensitivities of salinity and temperature have been found to be 215.744 nm/RIU and 0.519 nm/°C for the opto-microfluidic systems developed in this study. Considering the impact of the temperature perturbation to the phase shift, temperature calibration is proposed for a precise salinity measurement. The results demonstrate the practicability of opto-microfluidic devices for real-time salinity and temperature monitoring of sea water in harsh environment.

*Keywords:* opto-microfluidics, salinity, sea water, sensor, temperature

### 1. Introduction

Ocean is one of the most important ecologies on the earth which is crucial for the daily activities of human being. To preserve natural environment, environmental monitoring, including the measurement of water properties, must be carried out constantly (Shen et al., 2015; Urquhart et al., 2015; Forsythe et al., 2015; Xiao et al., 2015; Tan et al., 2015). Among different properties of oceans, temperature and salinity of sea water are two of the most important parameters for monitoring ocean currents, weather, iceberg floating, and oil pollution, which are critical for fishing, navigation, and human health. Various mechanical and electronic gauges have been fabricated using different techniques to achieve simultaneous measurement of different parameters. For example, the conductivity, temperature, and depth sensor (CTD) is a popular electronic instrument to measure the physical properties of seawater (Lawson et al., 2001). The gigantic volume of the testing equipment increases the energy consumption and cost. Fiberoptic sensors to achieve temperature and salinity measurement of seawater have been reported. The sensing elements mostly adopted fiber Bragg gratings (FBGs) (Shu et al., 2001; Men et al., 2008) and long period fiber gratings (LPGs) (Li et al., 2001; Wang et al., 2006), Mach-Zehnder interferometer (MZI) (Tian et al., 2008; Wang et al., 2010),

Fabry-Perot (FP) interferometer (Choi et al., 2010; Nguyen et al., 2011) and Michelson interferometer (Yuan et al., 2000). These fiber-optic sensing technologies exhibit significant advantages of flexibility and low fabrication cost. However, low salinity sensitivity of fiber sensors poses a major challenge for many applications. Therefore, design and fabrication of inexpensive, high-sensitive, miniaturized, and real-time sensors for oceanographic measurements are the most pressing demands.

Opto-microfluidics is a novel diagnostic technique which integrates optical components and microchannels on a palm-size chip to realize one or several measurements (Zhang et al., 2011). The significant advantages of opto-microfluidic sensors are portability, efficiency, sensitivity, versatile functionalities, compactness, minimized waste, and low cost. In these opto-microfluidic sensors, functional micro-optical structures are integrated with microchannels. The analyte in the microchannel interacts with the structures to generate different output signals. The reported micro-optical structures include diffraction grating (Schueller et al., 1999; Yu et al., 2010), MZI (Dumais et al., 2008; Crespi et al., 2010; Lapsley et al., 2011), ring resonance (Dai, 2009; Yebo et al., 2010; Zhang et al., 2011; Ren et al., 2012), surface plasmon resonance (Homola et al., 1997; Eftekhari et al., 2009), and LPG (Lor et al., 2005; Chin et al., 2008). Opto-microfluidics has been increasingly recognized as powerful technologies to realize environmental monitoring, biological analyses, and chemical syntheses.

In this paper, we report a waveguide-MZI based opto-microfluidic device for temperature and refractive index (RI) salinity measurement. By applying femtosecond lasers micro-

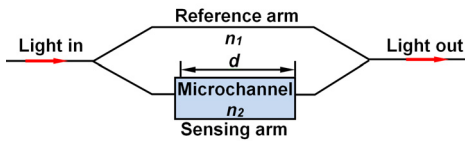
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fabrication technique in a photoresist material, a waveguide with a discontinuous core is fabricated and integrated into a microchannel as a miniaturized opto-microfluidic system. When the temperature or RI of the liquid in the microchannel varies, different phase shifts in the MZI allow determination of the salinity or temperature of the solution from the output spectra and light intensities of the MZI. According to the effect of the temperature and refractive index on the peak shift, accurate measurement of sea water salinity can be achieved.

## 2. Materials and Methods

### 2.1. Principles of Sensing

The Mach-Zehnder interferometer (MZI) is a device to detect the variation of the relative phase shift between two beams which are usually split from a single source. In opto-microfluidic devices, a MZI structure is typically integrated into an optical waveguide as shown in Figure 1. The signal is first coupled into the waveguide, and then split into two arms. One arm is a reference arm to compare the phase difference, and the other arm is used to sense the phase changes due to the variation of surround environmental parameters such as temperature (Dumais et al., 2008; Crespi et al., 2010), concentration (Lapsley et al., 2011), and refractive index (Densmore et al., 2008).



**Figure 1.** Schematic illustration of an opto-microfluidic MZI.

The output light intensity can be expressed as follow:

$$I = I_1 + I_2 + 2\sqrt{I_1 I_2} \cos(\delta\varphi) \quad (1)$$

where  $I$  is the output intensity,  $I_1$  and  $I_2$  are the intensities of the beams in the two branches, and  $\delta\varphi$  is the phase difference of the two beams.

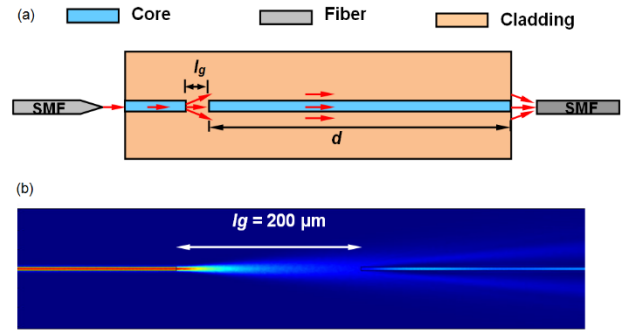
The phase difference is

$$\delta\varphi = \frac{2\pi(n_1 - n_2)d}{\lambda} \quad (2)$$

where  $d$  is the length of the microchannel,  $\lambda$  is the light wavelength,  $n_1$  and  $n_2$  are the refractive index of the materials in the two branches, respectively.

The schematic illustration of our MZI structure is depicted in Figure 2 (a). A waveguide with a discontinuous core is designed with the light coupled into the core from a taped SMF. When the light propagates into a gap, part of the light is re-coupled into the core, and the other part of light is scattered into the cladding. Then the light propagates along two different

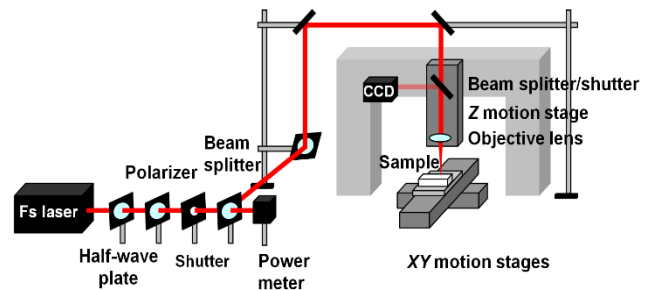
paths either the core or the cladding. A SMF collects the light comes out from the core and the cladding to generate interference. In this design, the core works as the reference arm and the cladding acts as the sensing arm. Two light paths are integrated into one simple waveguide structure which is super compact compared with typical MZI structures. Figure 2(b) shows a COMSOL simulation of light propagating in a MZI structure with a gap length  $l_g$  of 200  $\mu\text{m}$  and a core width of 4  $\mu\text{m}$  at the wavelength of 1561 nm. After the light passes the gap, the beams propagating along the cladding and core can be clearly observed.



**Figure 2.** (a) Schematic illustration of a MZI structure with a discontinuous core; (b) Simulation of light propagation in a MZI structure with a gap length of 200  $\mu\text{m}$  and a core width of 4  $\mu\text{m}$  at the wavelength of 1561 nm.

### 2.2. Device Fabrication

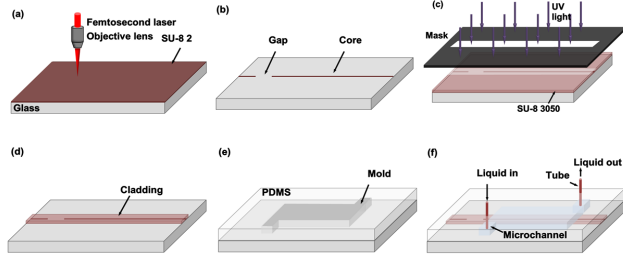
Figure 3 illustrates a typical microfabrication system with a femtosecond laser which is used in this study. The Ti:sapphire femtosecond laser with wavelength and repetition rate of 800 nm and 80 MHz, respectively, is focused on a sample by an objective lens (20 $\times$ , 0.46 NA). A variable attenuator, consisting of a half wave plate and a polarizer, is placed in the path of the beam to control and continuously adjust the output power of the laser. A shutter triggered by a computer program is used to control the exposure time of the sample to laser irradiation. A power meter monitors the change of the laser power in real time through a beam splitter.



**Figure 3.** Schematic illustration of a microfabrication system with a femtosecond laser.

Figure 4 shows the fabrication processes of a MZI chip. First, the photoresist material SU-8 2 (Microchem®) ( $n = 1.575$

at 1550 nm) is spin-coated and dried on a pre-cleaned glass substrate. Then the glass slide is put on the  $X, Y, Z$  translation stages (Aerotech®) which are controlled by a computer. A femtosecond laser (67 fs, 1.6 nJ pulses) is focused on the SU-8 2 film. By moving the  $X, Y, Z$  translation stages, a discontinuous core is written on the film. After baking and developing processes, the discontinuous core structure is shown on the glass slide. Photoresist SU-8 3050 (Microchem®) ( $n = 1.559$  at 1550 nm) is spin-coated and dried on the glass substrate again and exposed with an ultraviolet (UV) light through a metal mask. After the second baking and developing step, the cladding is shown on the glass slide. A PDMS microchannel is duplicated by the soft lithography technique, punched access holes with a needle, and bonded with the waveguide via oxygen plasma treatment (PDC-001, Harrick Plasma). The glass substrate is cut into a small piece and inserted capillary to generate a MZI chip. The cross section of the core is usually  $4.15 \mu\text{m} \times 3.20 \mu\text{m}$  (width  $\times$  height), and the cladding size is  $125.00 \mu\text{m} \times 10.00 \mu\text{m}$ . Figure 5 (a) shows a morphology of a waveguide with a discontinuous core. The length of the gap is  $200.00 \mu\text{m}$ . Figure 5 (b) presents a morphology of a waveguide covered by a microchannel with a width of 1 mm. Figure 5 (c) is a photo of the MZI chip with a chip length of 2.70 cm and a microchannel length of 1.60 cm. A taped SMF with a focused spot size of  $2.50 \mu\text{m}$  (OZ® optics) couples light from an  $\text{Er}^{3+}$  dual-band broadband source (1520 nm - 1620 nm) into the core via butt coupling method. Because the size of the core is smaller than the core diameter of the single-mode fiber (10.00  $\mu\text{m}$  corning® SMF-28e), a SMF can simultaneously collect the light comes out from the core and cladding. Figure 5 (d) presents a near field image of the transmission light obtained by a CCD camera (Hamamatsu camera system) in which the bright dot in the middle is the light coming from the core, whereas the long bright line is the light coming from the cladding.

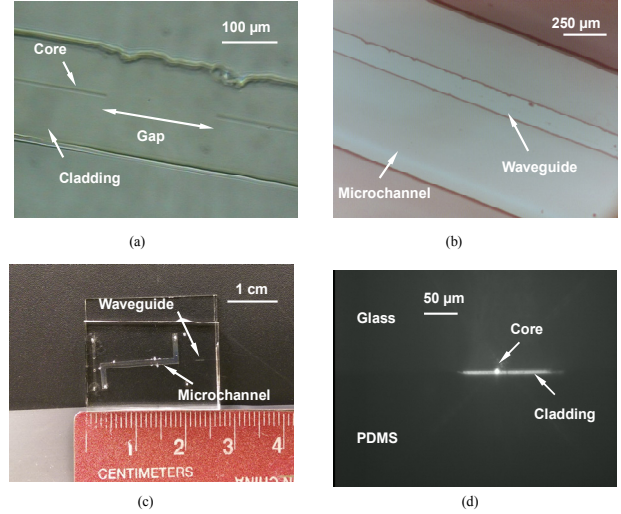


**Figure 4.** Procedures for MZI chip fabrication: (a) Femtosecond laser writing on the SU-8 2 film; (b) Discontinuous core; (c) Cladding fabrication with an UV light; (d) Waveguide with a discontinuous core; (e) PDMS microchannel fabrication; (f) MZI chip.

In this case, the Equation (2) changes to:

$$\delta\varphi = \frac{2\pi(n_{eff-co} - n_{eff-cl})d}{\lambda} = \frac{2\pi\Delta n_{eff}d}{\lambda} \quad (3)$$

where  $n_{eff-co}$  is the effective RI of the core,  $n_{eff-cl}$  is the effective RI of the cladding,  $\Delta n_{eff}$  is the RI difference of the core and cladding, and  $d$  is the length of the sensing arm.



**Figure 5.** (a) Morphology of a waveguide with a discontinuous core; (b) Morphology of the waveguide covered by a microchannel; (c) MZI chip; (d) Near field image of the transmission light obtained by a CCD camera.

When the phase difference satisfies the following condition:

$$\delta\varphi = 2m\pi \quad (4)$$

where  $m$  is the order of the MZI.

The attenuation peak or valley wavelength  $\lambda_m$  can be expressed as:

$$\lambda_m = \frac{\Delta n_{eff}d}{m} \quad (5)$$

Liquids with different RIs can be injected into the microchannel. As a result, the effective RI of the cladding varies accordingly. However, the effective RI of the SU-8 core is hardly affected by the liquid. Therefore, Equation (5) can be shown as:

$$\begin{aligned} \delta\lambda_{m,n} &= \lambda_{m,n'} - \lambda_{m,n} = \frac{(\Delta n_{eff,n}d + \delta n_{eff,n}l)}{m} - \frac{\Delta n_{eff,n}d}{m} \\ &= \frac{\delta n_{eff,n}l}{m} = \frac{\delta n_{eff,n}\lambda}{\Delta n_{eff,n}} \frac{l}{d} \end{aligned} \quad (6)$$

where  $\delta n_{eff,n} = n'_{eff-cl} - n_{eff-cl}$ , and  $l$  is the length of the microchannel.

If the environmental temperature of the waveguide rises, both the effective RIs of the cladding (SU-8 3050) and the core (SU-8 2) modes change to different extents ( $\delta n_{eff,T}$ ) due to the fact that the cladding and core have different thermo-optic coefficients. The attenuation peak wavelength shift  $\delta\lambda_{m,T}$  is:

$$\begin{aligned} \delta\lambda_{m,T} &= \lambda_{m,T'} - \lambda_{m,T} \\ &= \frac{(\Delta n_{eff,T} + \delta n_{eff,T})d}{m} - \frac{\Delta n_{eff,T}d}{m} = \frac{\delta n_{eff,T}d}{m} \end{aligned} \quad (7)$$

where  $\delta n_{eff,T} = (dn/dT_{core} - dn/dT_{cladding})Tdn/dT$  is the thermo-optic coefficient of the material.

Therefore, the shift in the peak wavelength can be expressed as:

$$\begin{aligned} \delta\lambda_{m,T} &= \frac{\left(\frac{dn}{dT_{core}} - \frac{dn}{dT_{cladding}}\right)d}{m} \\ &= \frac{\left(\frac{dn}{dT_{core}} - \frac{dn}{dT_{cladding}}\right)\lambda}{\Delta n_{eff,T}} T \end{aligned} \quad (8)$$

### 3. Results and Discussion

A chip with a gap length of 200.00  $\mu\text{m}$  is used to measure the refractive index and temperature. The core size is 4.15  $\mu\text{m} \times 3.20 \mu\text{m}$ , and the cladding size is 125.00  $\mu\text{m} \times 9.88 \mu\text{m}$ . The sensing arm is 24.29 mm and the microchannel has a size of 16.00 mm  $\times$  1.00 mm  $\times$  75.00  $\mu\text{m}$  (length  $\times$  width  $\times$  height). Figure 6 shows a transmission spectrum in the range of 1520 nm  $\sim$  1620 nm with salient interference patterns. For temperature sensing, the chip is placed on a small hotplate, and heated step by step. Transmission spectra are recorded and compared. Figure 7 presents the peak shift (red shift) at different temperatures, which exhibits a sensitivity of 0.519 nm/ $^{\circ}\text{C}$ . By maintaining the temperature of hotplate at 20  $^{\circ}\text{C}$ , saline solutions are infused into the microchannel one by one. Figure 8 shows the peak shift (blue shift) at different RI and the dependence of the peak shift on refractive index/salinity with a refractive index sensitivity of -215.744 nm/RIU.

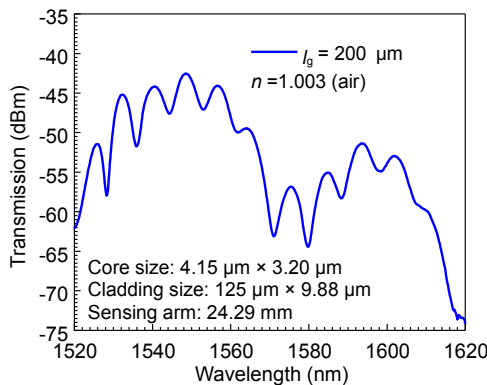


Figure 6. Transmission spectrum at the room temperature.

Following the sensing response with simultaneous variations in temperature and salinity, the total wavelength shift can be expressed as:

$$\Delta\lambda = 0.519\Delta T - 215.744\Delta n \quad (9)$$

where  $\Delta T$  is the change of the temperature, and  $\Delta n$  is the change of the refractive index. Since the wavelength shift exhibits a strong dependence on temperature, refractive index/salinity

sensing must be accompanied by a temperature calibration in order to obtain precise results. The final RI of the saline solution can be calculated by Equation (9) if the temperature is known.

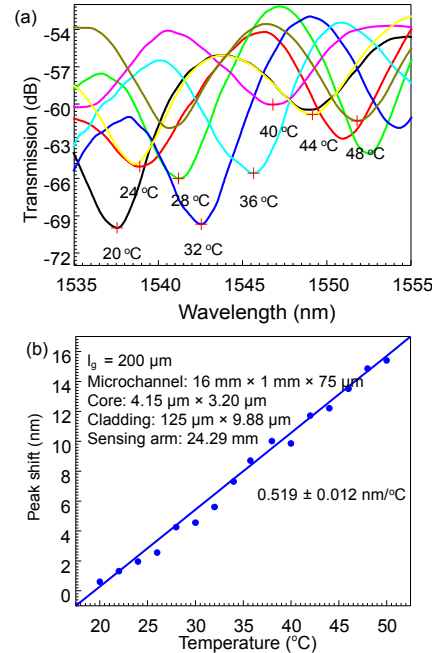


Figure 7. Temperature sensing: (a) Transmission spectra at different temperatures; (b) Dependence of the peak shift on temperature.

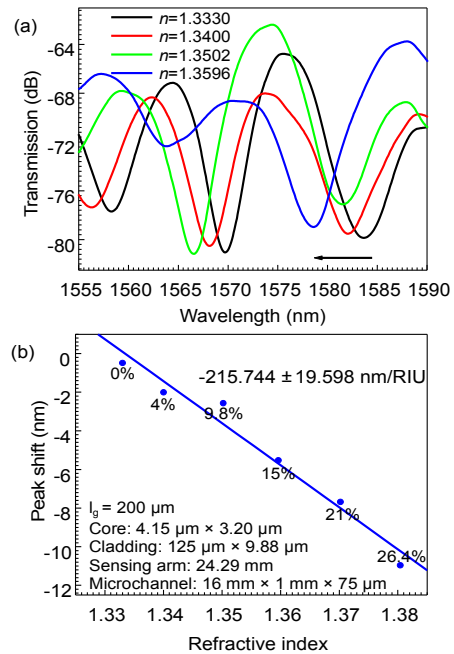
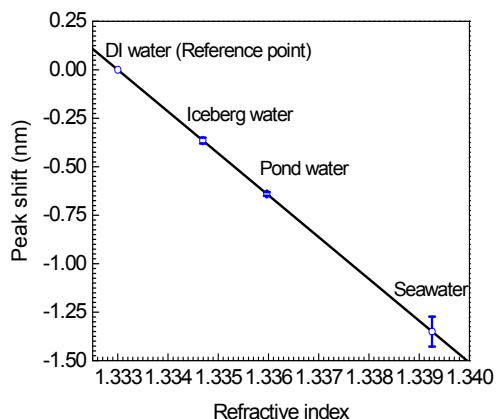


Figure 8. Refractive index sensing: (a) Transmission spectra at different RIs; (b) Dependence of the peak shift on refractive index/salinity.



**Figure 9.** Refractive index measurement of different water samples.

In order to prove the validity of the chip, water samples are introduced into the chip, including melted iceberg water, pond water, and sea water. By maintaining the temperature of hotplate at 20°C, distilled water is first infused into the chip for reference, and then water samples are injected into the micro-channel. Figure 9 shows the experimental results of these samples. The RI of iceberg is about 1.3347 which is a bit higher than DI water. The RI of the pond water is 1.3360. The RI of the seawater is about 1.3393. By calculation following the method discussed by Quan (Quan et al., 1995), the salinity is about 32.578‰, which is reasonable for the seawater.

#### 4. Conclusions

In summary, we have successfully designed and fabricated an opto-microfluidic MZI sensor based on a waveguide with a discontinuous core. Temperature and refractive/salinity measurement have been achieved. The temperature and refractive index sensitivities are 0.159 nm/°C and -215.744 nm/RIU, respectively, which are much higher than those of fiber-optic sensors (0.0102 nm/°C and 0.0165 nm/M in Men et al., 2008; 0.029 nm/°C and 0.069 nm/ppt in Wang et al., 2006). This device can be applied to measure any solution with a refractive index smaller than 1.559, which is the refractive index of the cladding material. Different water samples are tested using this chip with good agreement, which demonstrates the practicality of the opto-microfluidic devices for *in situ* salinity monitoring of sea water with high sensitivity, accuracy and low cost.

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